



## Original Article

## A deep learning risk prediction model for overall survival in patients with gastric cancer: A multicenter study



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## ABSTRACT

**Background and purpose:** Risk prediction of overall survival (OS) is crucial for gastric cancer (GC) patients to assess the treatment programs and may guide personalized medicine. A novel deep learning (DL) model was proposed to predict the risk for OS based on computed tomography (CT) images.

**Materials and methods:** We retrospectively collected 640 patients from three independent centers, which were divided into a training cohort (center 1 and center 2,  $n = 518$ ) and an external validation cohort (center 3,  $n = 122$ ). We developed a DL model based on the architecture of residual convolutional neural network. We augmented the size of training dataset by image transformations to avoid overfitting. We also developed radiomics and clinical models for comparison. The performance of the three models were comprehensively assessed.

**Results:** Totally 518 patients were prepared by data augmentation and fed into DL model. The trained DL model significantly classified patients into high-risk and low-risk groups in training cohort ( $P$ -value  $< 0.001$ , concordance index (C-index): 0.82, hazard ratio (HR): 9.79) and external validation cohort ( $P$ -value  $< 0.001$ , C-index: 0.78, HR: 11.76). Radiomics model was developed with selected 24 features and clinical model was developed with three significant clinical variables ( $P$ -value  $< 0.05$ ). The comparison illustrated DL model had the best performance for risk prediction of OS according to the C-index (training: DL vs Clinical vs Radiomics = 0.82 vs 0.73 vs 0.66; external validation: 0.78 vs 0.71 vs 0.72).

**Conclusion:** The DL model is a powerful model for risk assessment, and potentially serves as an individualized recommender for decision-making in GC patients.

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Gastric cancer (GC) is one of the most common gastrointestinal malignancies worldwide. Although its incidence has decreased, GC still serves as the third leading cause of cancer-associated deaths, particularly in Eastern Asia [1]. Currently, patients with advanced GC are recommended to receive surgical resection, adjuvant chemotherapy and radiotherapy for improvement of the treatment in line with the US National Comprehensive Cancer Network

guidelines [2]. However, previous studies revealed that the rates of 5-year survival are still poor, and surgical morbidity is high [3], which have led to wide investigation for survival analysis.

The state-of-the-science tumor-node-metastasis (TNM) staging system (8th edition) of GC promulgated by The American Joint Committee on Cancer (AJCC) is widely used as the gold standard for prognostic evaluation and survival risk stratification [4]. However, the authors indicated that the manual is not an exact science, which is the ongoing work and will be updated to reflect the state-of-the-art changing [4]. Particularly, for personalized medicine, The AJCC Personalized Medicine Core (PMC) committee has been increasingly conscious of the necessity for more individualized predictions than those presented by ordinal cancer staging systems based on risk models constructed by machine learning approach [5]. Overall survival (OS) was required by The AJCC PMC as the outcome being predicted for the risk models.

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Recently, related works have focused on non-invasive methods of imaging, especially for computed tomography (CT), which is the routinely used modality for staging and risk assessment [6]. Radiomics, an emerging field, is an accepted method to analyze the medical images by extracting amounts of quantitative features [7]. Previous study found that radiomic features extracted from CT images had prognostic value for overall survival in patients with lung cancer [8]. Zhang et al. developed a radiomic nomogram to predict early recurrence in GC patients following curative resection [9]. Some studies have demonstrated that radiomics method was a meaningful tool associated with tumor prognosis in patients with nasopharyngeal cancer and gastric cancer [10,11]. Nevertheless, standard procedures of radiomics method need accurate delineation for segmentation and retest the stability for features, which may cause variability and inconsistent reproducibility [12]. Thus, it is relatively convenient and labor-saving to develop a tool for survival analysis, which can lower the delineation standard and tailor training process to train the model by feeding segmented CT images into the network and extracting the features by itself [13].

Currently, studies on medical image analysis are undergoing a transformation from engineering of feature extraction to self-learning. In particular, deep learning (DL), a state-of-the-art methodology, has attracted much attention and achieved huge breakthroughs in a wide range of computer vision task and clinical applications [14]. Bello et al. demonstrated DL method can be applied to develop a motion model to efficiently predict survival [15]. DL method has been also used for the screening the GC patient focusing on endoscopic image-based analysis [16]. However, the implement of DL method for the risk prediction of OS in GC patients based on CT images remains unclear.

In this study, we developed a DL model for risk prediction of OS based on the widely recognized residual convolutional neural network (CNN) [17]. We also constructed a potential individualized recommender system to provide recommendations for decision-making.

## Materials and methods

Fig. 1 shows an overview of this study via the DL model in combination with the TNM staging system for the individualized treatment.

### Patients

Ethical approval was respectively received for the Institutional Review Board of each center, and informed consent from patients was waived. This was a retrospective multicenter study. A total of 640 consecutive patients who were pathologically diagnosed with GC from June 2010 to April 2019 were enrolled from three independent centers. We divided eligible patients into a training cohort ( $n = 518$ , from center 1 and center 2) and an external validation cohort ( $n = 122$  from center 3), which is shown in Supplementary Fig. A1. Supplementary Table A1 and Part 2 show the parameters for CT images and the details of follow-up for OS. Characteristics in the training and external validation cohorts are shown in the Table A2.

### Image segmentation

We used the software ITK-SNAP for segmentation [18]. For each patient, we selected a slice of CT image with largest tumor region and nearest upper and lower slices in portal venous phase by two experienced radiologists and outlined them with three rough rectangle boxes. In order to avoid coarse label for each patch, the region of interest was acquired at first. Afterwards, the input image for the deep learning model was the region of interest. For

constructing the radiomics model, we manually delineated precisely the tumor region of the slice with largest tumor region again. The diagram of segmentation is shown in Fig. 2.

### Model construction

We constructed a DL model based on 18-layers residual CNN with the input of segmented CT images (size:  $224 \times 224$ ) [17]. The model consisted of 8 residual blocks, which have the “short cut” for transmitting gradient efficiently and accelerating the convergence of the network (Fig. 2). We tailored the dense and dropout layers at the top of the model. We also defined the specialized loss function (Supplementary Formula A1) to train the model for risk prediction. Some techniques including data augmentation and fine-tuning were used to train the model and avoid overfitting. More details regarding the training procedure can be found in the Supplementary Part 4. For comparison, we also constructed the radiomics model (Fig. 2B) based on hand-crafted features and clinical models for comparison. The output of each model, named risk score for each GC patient, represented the hazard degree for occurrence of the endpoint of interest.

### Assessment of prognostic performance for DL model

To investigate the potential association between the proposed DL model and OS, we depicted Kaplan–Meier (KM) curves. For each patient, the cutoff of median risk score was obtained in the training cohort. Patients with the scores lower than the cutoff were classified into the low-risk group, while others were classified into the high-risk group.

Furthermore, we performed stratification analysis to validate the performance of the DL model in different subgroups (T stage, N stage, TNM stage, and adjuvant chemotherapy). We employed visualization techniques to present the self-learned feature maps inside the DL model [19]. We developed a risk score grading tool based on a widely used nomogram [20]. To show the network benefit, the clinically accepted tool of decision curve analysis (DCA) was applied to verify the prognostic value of the DL model [20]. We calculated the Harrell’s concordance index (C-index) and hazard ratio (HR) to evaluate the performance of the three models. Finally, we proposed an individualized recommender system for potential clinical application.

### Statistical analysis

We performed the statistical analysis with R software (<http://www.R-project.org>). The features and clinical variables were compared using the Mann–Whitney  $U$  test. KM curves were compared by Log-Rank test. Moreover, the G-rho rank test was used for calculation of the HR [21]. We also compared the C-index of the DL model with other models by a non-parametric test. The result was considered statistically significant when the  $P$ -value (from two-sided tests) was less than 0.05.

## Results

Schoenfeld residuals test demonstrated that each clinical variable was eligible to use Cox regression for univariable and multivariable analysis (Fig. A2). T stage, N stage, and adjuvant chemotherapy were significant ( $P$ -value  $< 0.05$ , Table A3) for construction of clinical model. In training cohort, median survival time was 28 months. In external validation cohort, the median survival time was 56 months.

The DL model with residual blocks and the identity mapping was constructed to show the learning capability of risk prediction. A total of 12,432 images were generated by data augmentation and

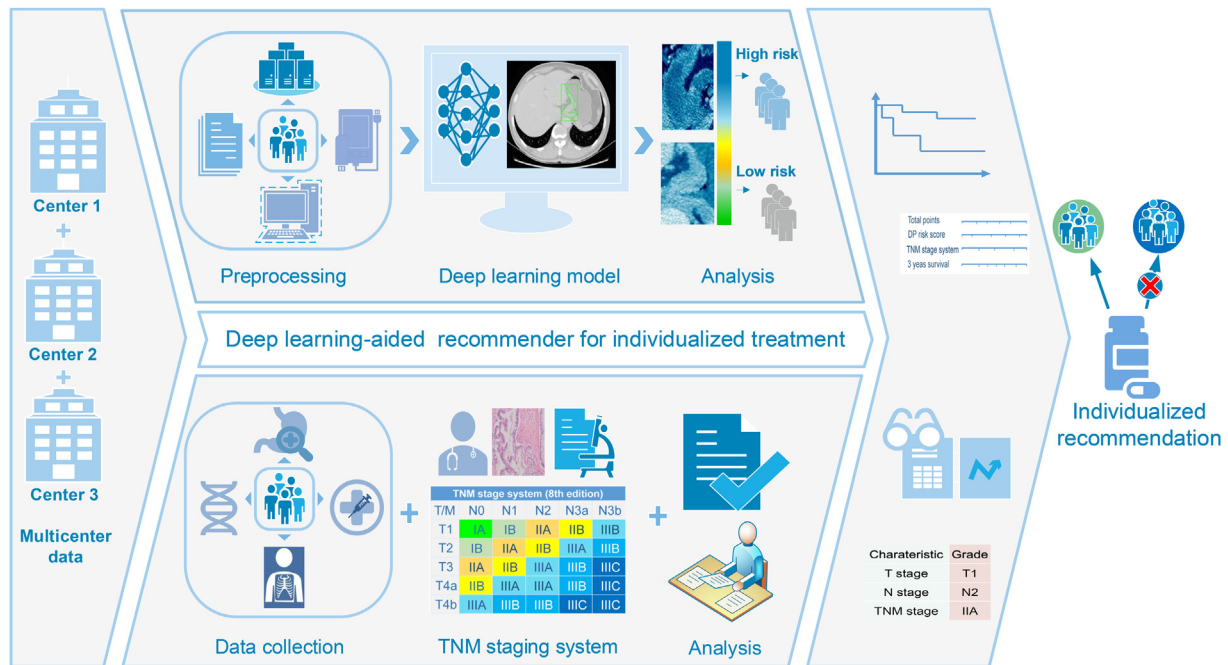


Fig. 1. The overview of the study design.

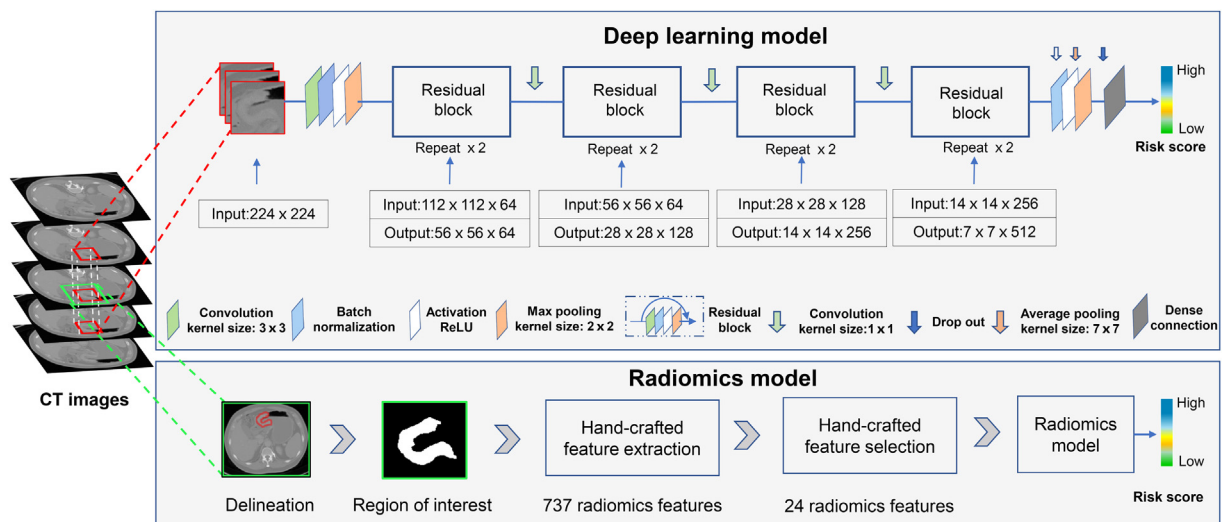


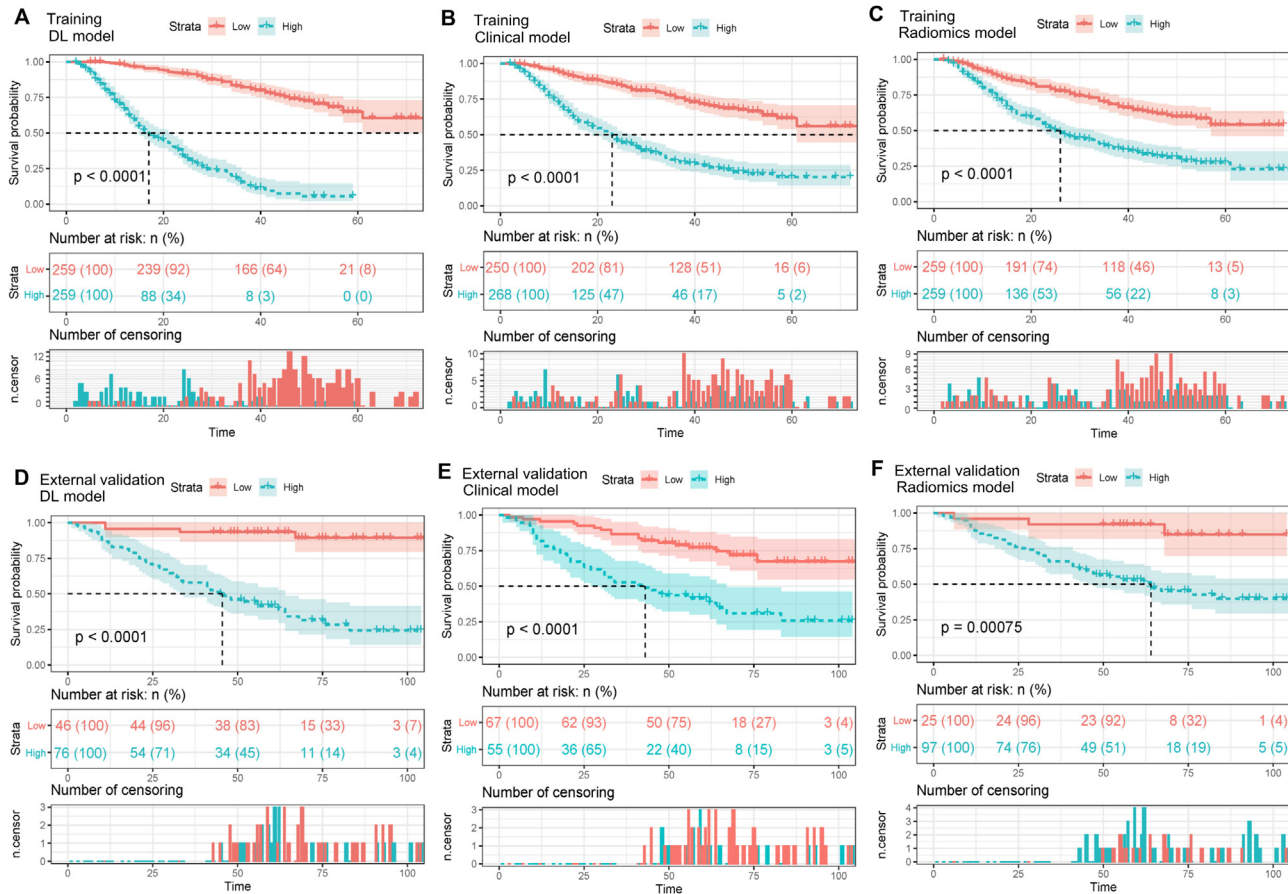
Fig. 2. Architectures of deep learning (DL) model based on residual convolutional neural network and radiomics model based on hand-crafted features.

fed into DL model. Finally, the risk score was output for each patient. Further details regarding the development of the radiomics model are shown in Supplementary Part 7.

The DL model could classify all patients into two different risk subgroups (the low-risk and high-risk) in the training cohort ( $P$ -value  $< 0.001$ , C-index: 0.82, 95% confidence interval (CI) 0.80–0.84, HR: 9.79, 95%CI 7.15–13.41) and external validation cohort ( $P$ -value  $< 0.001$ , C-index: 0.78, 95%CI 0.72–0.83, HR: 11.76, 95%CI 4.23–32.71). KM curves for DL model are shown in Fig. 3. Clinical data analysis of different risk groups in the both cohorts are shown in Table 1. In the training cohort, median survival time was 14 months in the high-risk group, and 45 months in low-risk group. In the external validation cohort, the median survival time in the high-risk group was 45 months, and 66 months in low-risk group. The stratification analysis revealed that the DL model

also had good performance for risk prediction in different subgroups pertaining to N stages (Fig. A3), T stages (Fig. A4), TNM stages (Fig. A5), and adjuvant chemotherapy (Fig. A6).

DL model could learn discriminative features for GC patients in different risk groups with different survival time. Examples for two patients were shown in the Fig. 4, one from the high-risk group and one from the low-risk group in line with the risk scores predicted by the three models. The feature maps extracted from shallow to deep layers of the DL model were visualized. Highly responsive areas colored red of a region of interest (ROI) were found the different in two risk groups. With the number of layers of the network increasing, the DL model can focus on the highlights in the ROI with small sized feature maps by convolution and pooling. The high-risk groups with corresponding risk scores (DL vs Clinical vs Radiomics: 0.98 vs 0.6 vs 0.62) and low-risk groups with



**Fig. 3.** Comparison of Kaplan–Meier (KM) curves for models. (A), (D): deep learning (DL) model; (B), (E): clinical model; (C), (F): radiomics model. Each vertical tick on the bottom of the KM curves represents a patient who was censored at that time.

corresponding risk scores (DL vs Clinical vs Radiomics: 0.1 vs 0.28 vs 0.49) were obtained by the three models.

Clinical data analysis in Table A2 shows that the HR for adjuvant chemotherapy was 0.62 (95% CI: 0.46–0.82), which revealed the adjuvant chemotherapy was a good prognostic factor for GC patients. DL model also showed consistent risk prediction by further stratification. According to the analysis of multiple factors of N stage and adjuvant chemotherapy, the further results (Fig. A7) shows that GC patients were also divided into high and low cumulative hazard subgroups by the DL model. We also found that the DL model can performed well according to the T stage and adjuvant chemotherapy (Fig. A8). In each subgroup, the findings showed that GC patients in low-risk groups with lower cumulative hazard grouped by DL model had better OS than the high-risk.

To evaluate the performance of the three models, the comparison for KM curves is shown in Fig. 3. The cut-off obtained in the training cohort was 0.668, 0.502 and 0.504 for the deep learning model, clinical model and radiomics model respectively. We depicted the distribution of risk scores for patients predicted by three models (Fig. 4A). In the distribution shape of the risk score for the DL model in the training cohort, all patients were divided into two subgroups, wherein patients in high-risk group were centralized. Moreover, in Fig. 4B and C, the DL model shows the best capability for prediction with the highest C-index in the training cohort (DL vs Clinical vs Radiomics: 0.82 vs 0.73 vs 0.66), wherein the comparison of C-index was significant ( $P$ -value < 0.01). Meanwhile, C-index of the DL model also outperformed the others in the external validation cohort (DL vs Clinical vs Radiomics: 0.78

vs 0.71 vs 0.72) with a significant difference between the DL model and the clinical model ( $P$ -value < 0.05).

As is shown in Fig. 4C, the DL model had the highest HR both in training cohort (9.79 vs 3.84 vs 2.48) and external validation cohort (11.76 vs 3.57 vs 5.86), which indicated the high-risk groups predicted by DL model had higher hazard of death than the high-risk groups predicted by other models. Furthermore, in comparisons of the time-dependent receiver operating characteristic (ROC) curves (1-year, 2-year and 3-year) for three models, we found that the performance of the DL model equally outperformed the other models in both cohorts (Fig. A9).

The nomogram, calibrations and DCA curves of DL model were depicted in Fig. 5, which shows good performance for risk prediction. The DCA indicated that the DL model provided a greater net benefit than other models for the patients. Therefore, we constructed the individualized grading rule of nomogram to divide GC patients into low-risk and high-risk subgroups. After all GC patients were divided into two groups by the individualized grading rule, we constructed a deep learning-aided recommender by calculating the difference ( $D_{\beta}(x) - D_{risk}$ ) to measure the degree of risk in the subgroups (Supplementary Fig. A10).

In order to show the generalizability of the model, we constructed deep learning (DL) model again, where we combined center 1 and 3 as the training cohort ( $n = 459$ ) and used center 2 as external validation cohort ( $n = 181$ ). As shown in the follow figure, the DL model significantly classified patients into high-risk and low-risk groups in training cohort (Supplementary Fig. A11,  $P$ -value < 0.001, concordance index (C-index): 0.77, 95% confidence



**Table 1**

Characteristics analysis by deep learning model.

Characteristic	Training cohort		P-value <sup>‡</sup>	External validation cohort		P-value <sup>‡</sup>
	Low risk	High risk		Low risk	High risk	
Age (years) <sup>†</sup>	57(56 ± 10)	59(56 ± 11)	0.14	59(59 ± 10)	58(58 ± 12)	0.77
Gender			0.86			0.74
Male	189(73)	188(73)		32(70)	52(68)	
Female	70(27)	71(27)		14(30)	24(32)	
Tumor localization			0.49			<0.01
Proximal	46(18)	54(21)		13(28)	33(43)	
Middle	68(26)	66(25)		5(11)	13(17)	
Distal	145(56)	139(54)		28(61)	30(40)	
Tumor size			0.02			<0.01
<5 cm	173(67)	116(45)		28(61)	23(30)	
≥5 cm	86(33)	143(55)		18(39)	51(67)	
NA				0(0)	2(3)	
Lymphovascular invasion			0.01			0.28
Negative	82(32)	49(19)		20(43)	31(41)	
Positive	177(68)	210(81)		26(57)	45(59)	
Differentiation			0.05			0.13
Well + moderate	127(49)	89(34)		17(37)	25(33)	
Poor + undifferentiated	132(51)	170(66)		29(63)	51(67)	
T stage			<0.01			<0.01
T1a-T1b	22(8)	1(0)		3(6)	2(2.5)	
T2	48(19)	12(5)		7(15)	2(2.5)	
T3	113(44)	88(34)		32(70)	57(75)	
T4a	76(29)	158(61)		4(9)	15(20)	
N stage			<0.01			<0.01
N0	108(42)	35(14)		10(22)	14(19)	
N1	58(22)	29(11)		15(33)	10(13)	
N2	39(15)	67(26)		9(19)	20(26)	
N3a-N3b	54(21)	128(49)		12(26)	32(42)	
TNM stage			<0.01			<0.01
I	40(15)	6(2)		7(15)	2(3)	
II	82(32)	29(11)		19(41)	23(30)	
III	137(53)	224(87)		20(44)	51(67)	
Adjuvant chemotherapy			<0.01			0.63
No	47(18)	61(24)		25(54)	37(49)	
Yes	212(82)	198(76)		21(46)	39(51)	
Follow-up (Month) <sup>†</sup>	45(43 ± 14)	14(17 ± 11)		66(67 ± 21)	45(45 ± 27)	

Values in parentheses are percentages (%).

<sup>†</sup> Values are median(mean + std).<sup>‡</sup> Continuous variables were tested by Mann–Whitney *U* test and discrete variables were tested by Pearson's Chi-squared test.

interval (CI):0.74–0.79, hazard ratio (HR): 5.54, 95%CI: 4.07–7.54) and external validation cohort (*P*-value <0.001, C-index: 0.76, 95%CI 0.71–0.80, HR: 6.91, 95%CI 4.06–11.78).

## Discussion

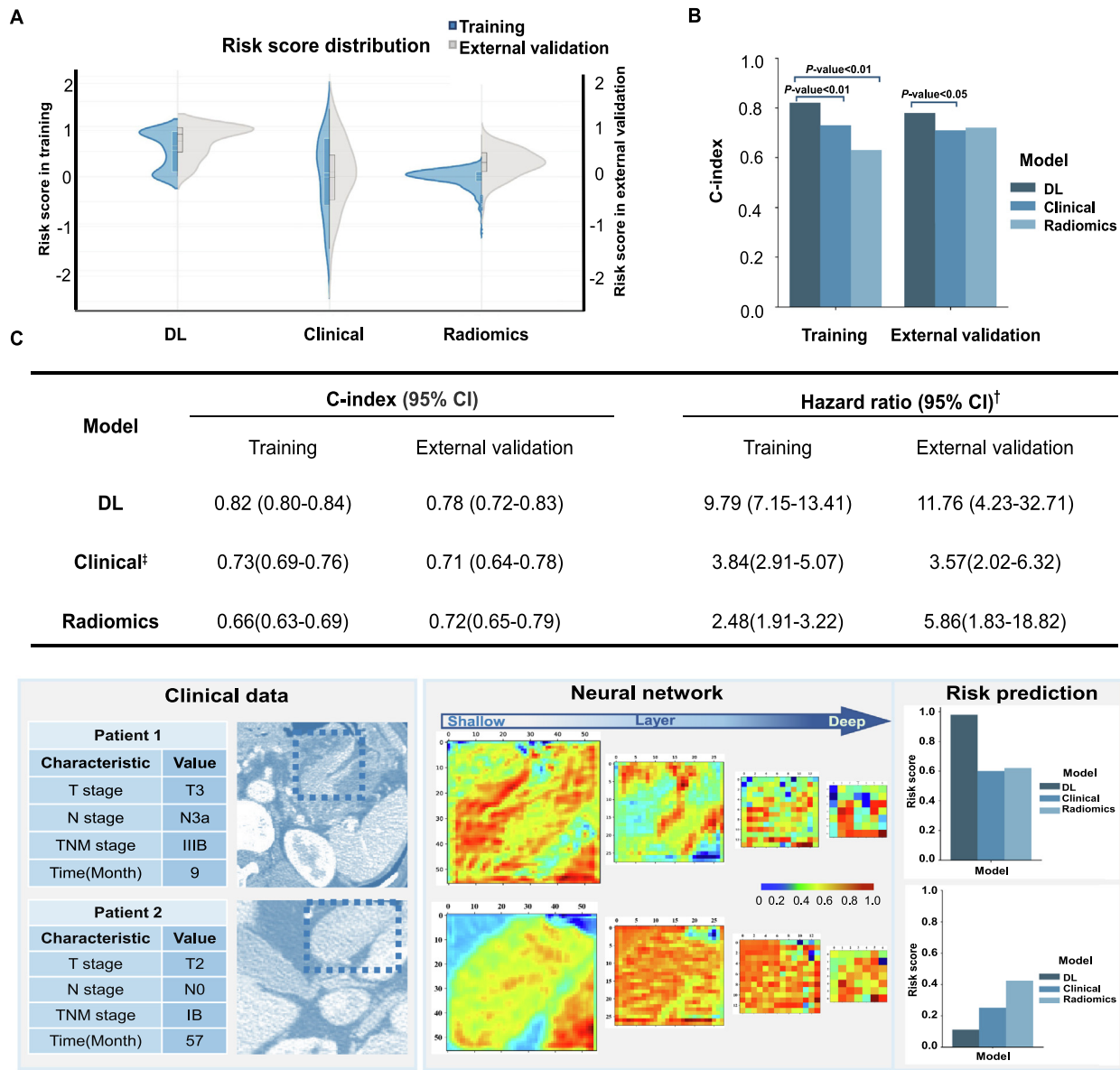
In this study, we investigated the performance of a DL model using CT images, with the aim of improving the prediction of OS for GC patients. The DL model showed encouraging outcomes with regard to its capability to stratify GC patients into two groups with discrepant prognosis in the training and external validation cohorts compared with other models. We found that high-risk groups had poor OS, whereas low-risk groups better. To further visualize and interpret the dynamic change inside the DL model, feature maps were vividly visualized and represented. For the standard treatment of adjuvant chemotherapy, covariate analysis for the DL model shows potential guidelines for GC patients.

We proposed a DL model based on residual network, which was demonstrated that it was suitable to predict the risk for GC patients. We implemented several methods to train the model (Supplementary Part 4). He et al. have demonstrated that residual block and the identity mapping can improve the learning capability, and address the degradation problem [17]. Our outcomes revealed that residual network, in some cases, could also address the degradation problem for CT images analysis, and data augmentation was useful for enlarging the training data to cope with the

problem of overfitting. Meanwhile, the techniques of dropout and fine-tuning were also efficient to improve the robustness for the DL model based on limited CT images.

Although the golden standard for treatment of GC patients is AJCC TNM staging system [4], the AJCC has realized that risk model for OS is necessary for more individualized probabilistic prognostication [5]. In particular, for personalized treatment, previous studies have implicated that the TNM staging system have some drawbacks [22]. For instance, although the patients belonged to confirmed subgroup (T stage = T2, N stage = N0, TNM stage = IB), we can't obtain the further information about degree of risk for each patient or the different risk groups they belonged to, which may lead to suboptimal recommendations for individualized treatment. Conversely, the DL model can classify the patients into different risk groups and the recommender provides recommendation for individualized treatment combined with TNM staging system. According to the stratification analysis with multiple factors of the N stage, T stage, and adjuvant chemotherapy, the findings revealed that the DL model is a powerful predictor for risk prediction, which have the potential to serve as a model-based reference index for an updating TNM staging system to improve clinical decision making.

Currently, the popular method of radiomics plays an important role in prognostic analysis [23]. However, elaborate delineation by radiologists of the ROI hinders deployment of segmentation in clinical practice. In practice, the work of segmentation for our proposed model is easy and time-saving to complete, since we do

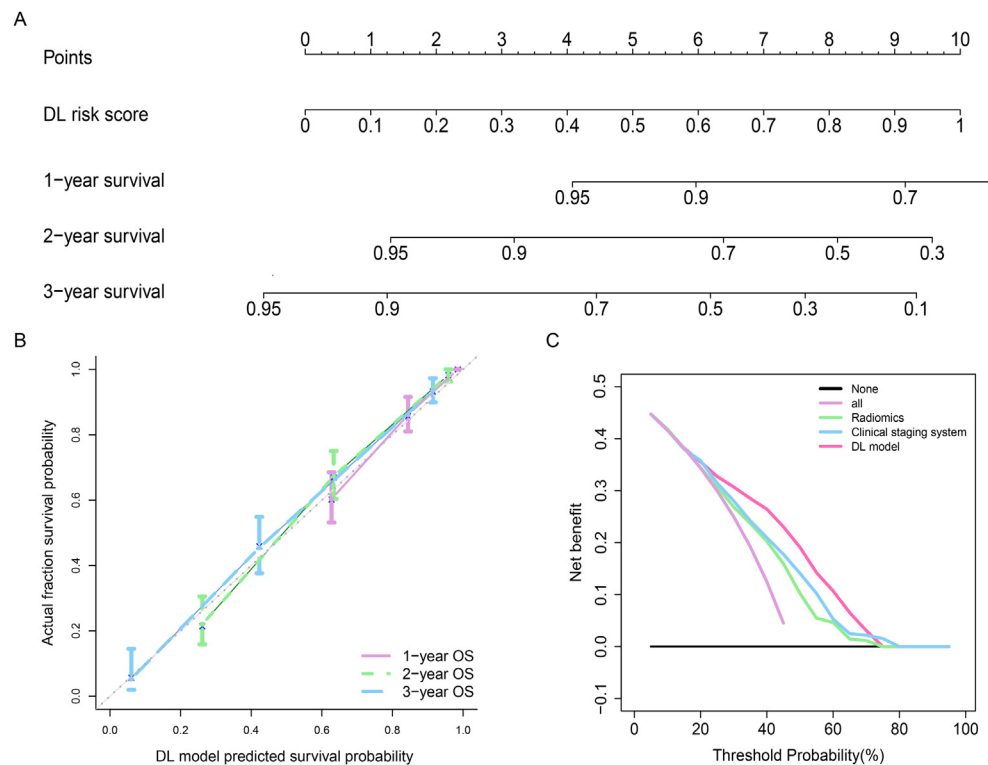


**Fig. 4.** Model analysis with measurable indicators. (A) Risk score distribution for the origin output of three models; (B) Comparison of the C-index between deep learning (DL) models and other models by *P*-value. The Student's *t*-test by R package ("survcomp", version:1.34.0) used for the comparison of the concordance indices; (C) Comparison of model performance by concordance index (C-index) and hazard ratio (HR). (D) Model interpretation and visualization for the potential association between feature maps with pathological staging information. <sup>†</sup> The HR was calculated by comparing the high-risk group with low-risk group. <sup>‡</sup> The clinical model was constructed based on AJCC 8th staging system in combination with the risk factors of adjuvant chemotherapy.

not require the tumor to be precisely delineated. Hence, the DL model is considered relatively as an easy-to-use and labor-saving tool for clinical application. In addition, compared with hand-crafted radiomics features, the feature maps were learned automatically from the shallow to deep convolutional layers by the DL model, including simple low-level features to complex high-level features. Hence, our study presents a promising approach.

In addition, Cox Proportional Hazard (CPH) Model are widely used for survival analysis [24]. However, the assumption of CPH model that logarithmic HR is linearly correlated with each risk factor is restrictive. While universally-applicable methods, such as DL method, can construct robust model without any assumption. Katzman et al. illustrated that DL model (DeepSurv) showed good performance and can provide personalized recommendations based on simulated and real survival data [25]. Yousefi et al.

reported that DL model showed good performance to learn information from diseases for survival analysis with public molecular data [26]. Kim et al. applied the DeepSurv for survival analysis in oral squamous cell carcinoma (SCC) patients, and the model outperformed the random survival forest (RSF) and the CPH models [27]. Matsuo et al. investigated 40 clinical features and indicated that DL model can be a potential tool for survival prediction in women with cervical cancer, which showed superior performance than CPH model [28]. Sun et al. proposed a multimodal DL model by integrating Multi-dimensional Data (clinical and gene) for the prognosis prediction of breast cancer, and achieved a better performance than other existing methods with single-dimensional data [29]. Nie et al. constructed a 3D DL model for feature extraction with multi-modality brain images of glioma patients, and experimentally found that the DL method could learned discriminative



**Fig. 5.** Clinical application and further validation for deep learning (DL) model. (A) Individualized grading rules for risk score based on nomogram. (B) Calibration curves of the DL nomogram in the training cohort. (C) Comparison of decision curve analysis for the DL model.

features from multi-modality images for accurate prediction of the OS time [30]. Previous study exploited a multi-channel 3D CNN model to extract self-learned features from multi-modal brain images [31]. They found multi-channel deep survival network is powerful for prediction of OS time. Yao et al. proposed a deep correlational survival model to handle multi-modality data effectively, and the result demonstrated that the learned interactions can affect survival outcomes [32]. We also demonstrated that DL model outperformed the model constructed based on hand-crafted features and the clinical model based on clinical risk factors.

Despite the encouraging performance of the DL model, there are several limitations. Our model was developed based on the patients of Asian race, and further validation across other races should be studied. Although the segmentation was time-saving for the point of the comparison, the work has defects. The further work should be done for comparison to show the advantage of deep learning method for survival model. Meanwhile, the DL model was demonstrated here with only a limited dataset, and a larger dataset should be collected to validate a more robust performance. Additionally, the model was constructed only based on preoperative CT images, which may show more significant findings in combinations with pathological image and other types. We only employed three slices in each patient to construct model. Although three-dimensional delineation is time-consuming, the further work should be explored. Above all, although the work of interpretation and visualization was shown, the more acceptable and friendly approach for interpretability should be investigated.

In conclusion, the DL model can provide CT-based prognostic risk scores related to the OS of GC patients, and the findings demonstrated higher prognostic value than clinical and radiomics models. Most notably, our individualized recommender based on the DL model was validated through diverse verification, wherein it showed powerful prognostic ability. Therefore, the recommender

is a potential tool to assist clinicians with therapeutic decision-making and individualized treatment.

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### Declaration of interests

The authors declare no potential conflicts of interest.

### Appendix A. Supplementary data

Supplementary data to this article can be found online at <https://doi.org/10.1016/j.radonc.2020.06.010>.

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